Effect of High- and Low-molecular-weight Low-substituted Hydroxyethyl Starch on Blood Coagulation during Acute Normovolemic Hemodilution in Pigs

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Background: Hydroxyethyl starches (HES) with lower impact on blood coagulation but longer intravascular persistence are of clinical interest. The current study aimed to investigate in vivo the isolated effect of molecular weight on blood coagulation during progressive acute normovolemic hemodilution.

Methods: Twenty-four pigs were normovolemically hemodiluted up to a total exchange of 50 ml · body weight-1 of HES 650/0.42 or HES 130/0.42. Serial blood sampling was performed to measure HES plasma concentration and to assess blood coagulation. Concentration–effect relations were analyzed by linear regression, followed by the Student t test on regression parameters.

Results: Blood coagulation was increasingly compromised toward hypocoagulability by acute normovolemic hemodilution with both treatments (P < 0.01). Significantly greater impact on activated partial thromboplastin time (P = 0.04) and significantly stronger decrease of maximal amplitude (P = 0.04), angle α (P = 0.02), and coagulation index (P = 0.02) was seen after acute normovolemic hemodilution with HES 650/0.42 as compared with HES 130/0.42. Except for factor VIII (P = 0.04), no significant differences between both treatments were observed when relating antihemostatic effects to HES plasma concentrations (P > 0.05). A significantly lesser decrease of hemoglobin concentration has been found with HES 650/0.42 as compared with HES 130/0.42 (P < 0.01) in relation to HES plasma concentrations.

Conclusion: High-molecular-weight HES (650/0.42) shows a moderately greater antihemostatic effect than low-molecular-weight HES (130/0.42) during acute normovolemic hemodilution. However, similar effects on hemostasis were observed with both treatments when observed antihemostatic effects were related to measured HES plasma concentrations. In addition, HES 650/0.42 may have a lower efficacy in immediately restoring plasma volume.

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Received from the Department of Anesthesiology, University Hospital of Lausanne and University of Lausanne, Lausanne, Switzerland. Submitted for publication January 10, 2006. Accepted for publication July 31, 2006. Supported by departmental funds and B. Braun Medical SA, Crissier, Vaud, Switzerland. The funding by B. Braun was exclusively for the experiment and not personal. The publication of the current results did not require a formal authorization of the manufacturer but was discussed with all coauthors, including those being employees of B. Braun (Dr. Fisch and Burmeister). Drs. Burmeister and Fisch are employees of B. Braun AG, Melsungen, Germany, and Crissier, Switzerland, and Dr. Spahn is doing paid consulting for B. Braun Medical SA, Crissier, Switzerland. The Department of Anesthesiology of the University Hospital of Lausanne has done other research projects in collaboration with B. Braun AG, Melsungen, Germany, and Crissier, Switzerland, and has thereby received other funding in the past as well as educational funds from the competitor companies.

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HYDROXYETHYL starches (HES) are high-polymeric glucose compounds obtained by hydrolysis and subsequent hydroxyethylation from the waxy maize starch amylopectin. Mean molecular weight is a major determinant of the physicochemical characteristics of HES preparations. The latter characteristics are furthermore influenced by the molar substitution ratio, which expresses the average number of hydroxyethyl groups added per unit of glucose, and by their C2/C6 ratio, which refers to the site preference of hydroxyethylation at the glucose subunit carbon atoms occurring mainly at positions C2 and C6, and to a lesser degree at position C3.

Hydroxyethyl starch solutions are considered as effective plasma volume expanders with respect to their colloid oncotic properties and thus are widely used in clinical practice as plasma substitutes. However, the clinical use of HES is limited mainly by their potential to negatively affect hemostasis. Impaired platelet function, a type I von Willebrand–like syndrome with reduced levels of factor VIII (VIII) and von Willebrand factor (vWF) exceeding a mere hemodilution effect, as well as impaired coagulation measured by thromboelastography (TEG), Haemoscope Corporation, Niles, IL, have been reported. Because of several studies in patients undergoing cardiac surgery showing increased bleeding and transfusion requirements as well as higher mortality after administration of HES 450/0.7 (Hespan, DuPont Pharma, Wilmington, Germany), the US Food and Drug Administration has recently issued a warning against high-volume administration (> 20 ml/kg) of the latter HES solution. Previous studies investigating the antihemostatic effect of different HES solutions have considered molecular weight to be the crucial factor in determining the impact on hemostasis. However, this statement was limited by the fact that the reduction of molecular weight of the tested HES solutions has been associated with a concomitant reduction of molar substitution. Although a systematic investigation of the blood coagulation–compromising effect of molecular weight was lacking, the use of HES solutions with lower molecular weight and low molar substitution has been claimed to minimize the risk of coagulopathy. Contrary to the former assumptions, a recent study revealed similar alterations of blood coagulation when high-molecular low-substituted HES was compared with low-molecular low-substituted HES at equal molar substitution. Therefore, high-molecular low-substituted HES solutions may be expected to show an improved pharmacokinetic...
behavior with a prolonged initial half-life without an exaggerated compromise on blood coagulation.\textsuperscript{15}

Currently, the isolated effect of molecular weight on blood coagulation has been examined only after hypervolemic hemodilution and with relatively low doses (20 ml \textcdot kg\textsuperscript{-1} \textcdot body weight [BW]\textsuperscript{-1}).\textsuperscript{15} Less is known about the effects on \textit{in vivo} whole blood coagulation after intraoperative colloidal replacement of blood loss with high- and low-molecular-weight low-substituted HES solutions. The aim of this study was to investigate \textit{in vivo} the blood coagulation-promising effect of HES solutions of varying molecular weights (HES 650/0.42 vs. HES 130/0.42) at equal molar substitution (0.42) during progressive acute normovolemic hemodilution (up to 50 ml \textcdot kg\textsuperscript{-1} \textcdot BW\textsuperscript{-1}) in pigs.

Materials and Methods

The animal experiments were performed according to the guidelines of the Swiss Federal Veterinary Office. The protocol was approved by the Veterinary Office of the Canton of Vaud (Service Vétérinaire, Lausanne, Canton de Vaud, Switzerland). The study group consisted of 24 pigs with a mean BW of 43 ± 4 kg. The pigs were fasted overnight but allowed free access to water.

\textit{Animal Preparation}

At the time of their arrival at the laboratory, the animals received intramuscular premedication with 0.5 mg/kg xylazine (Rompun 2%; Bayer AG, Leverkusen, Germany), 20 mg/kg ketamine (Ketaminol 10; Veterinaria AG, Zurich, Switzerland), and 1 mg atropine (Atropinum sulf.; Sintetica S.A., Mendrisio, Switzerland). After the animals were sedated, anesthesia was induced by administration of 3% halothane (Halothane; Draeger, Lubeck, Germany), and 1 mg atropine (Atropinum sulf.; Sintetica S.A., Mendrisio, Switzerland), and 20 mg/kg ketamine (Ketaminol 10; Veterinaria AG, Zurich, Switzerland), and 1 mg atropine (Atropinum sulf.; Sintetica S.A., Mendrisio, Switzerland). After the animals were sedated, anesthesia was induced by administration of 3% halothane (Halothane; Dräger, Lübeck, Germany) by mask, followed by tracheal intubation.

Controlled ventilation was performed using tidal volumes of 10 ml/kg and a ventilatory rate adjusted to maintain alveolar carbon dioxide pressure at 35–40 mmHg (13–18 min\textsuperscript{-1}). The inspired oxygen fraction was maintained and monitored at 1.0 during surgical instrumentation. Thereafter, ventilation was continued with an inspired oxygen fraction of 0.4 (air-oxygen mixture). Anesthesia was maintained by means of 0.8–2.0% halothane based on heart rate and blood pressure response to surgical stimulation of each individual animal and left unchanged during the entire study. The car vein was cannulated (18-gauge cannula). Analgesia was guaranteed by administration of a continuous intravenous infusion of fentanyl (Sintetica S.A., Mendrisio, Switzerland) in a dosage of 4 μg \textcdot kg\textsuperscript{-1} \textcdot h\textsuperscript{-1} during the entire period of surgical instrumentation.

A catheter was placed into the internal jugular vein for normovolemic hemodilution, measurement of central venous pressure, and venous blood withdrawal for laboratory measurements. A further catheter was placed in the carotid artery, allowing continuous measurement of mean arterial blood pressure and blood withdrawal for arterial blood gas analyses. Via the contralateral carotid artery, an arterial cannula (AS10V; Jostra AG, Hirrlingen, Germany) was inserted and connected to a cardioplegia pump (SII Double Head Pump; Stöckert, Munich, Germany) for controlled withdrawal of blood for normovolemic hemodilution.

Further monitoring of the animals included continuous three-lead electrocardiogram, heart rate reading, and temperature monitoring. In addition, a direct bladder catheterization was performed for urine sampling.

\textit{HES Characterization}

Hydroxyethyl starch solutions with different molecular weights (647 and 136 kd) but identical molar substitution (0.42) as well as identical C2/C6 ratio (5:1) were investigated. To ensure full identity of molar substitution and hydroxyethylation pattern, both HES colloids were manufactured using the same raw HES preparation by successive hydrolysis. Thin-boiling waxy maize starch was suspended in water, activated by means of sodium hydroxide, and allowed to react with ethylene oxide for 2 h at 40°C. The amounts of waxy maize starch and ethylene oxide were chosen to yield HES with a molar substitution of 0.42. This original HES with its unique hydroxyethylation pattern was stepwise hydrolyzed thereafter by means of treatment with hydrochloric acid to yield final HES solutions with molecular weights of 647 kd (HES 650) and 136 kd (HES 130). These were treated with activated carbon, purified by ultrafiltration, diluted to a final concentration of 6% (wt/vol) in isotonic saline, filled in glass bottles of 500 ml each, and heat-sterilized at 121°C for 20 min. For determination and verification of HES molecular weights, HES sample solutions were analyzed in duplicate by gel permeation chromatography–multiangle laser light scattering (GPC-MALLS; Wyatt Technology, Woldert, Germany) at a flow rate of 1 ml/min in 70 mM phosphate buffer, pH 7.0, using serial gel permeation chromatography columns HEMA Bio 40, 100, and 1000 (PSS, Mainz, Germany). Mean average molecular weight was calculated using Astra software (Wyatt Technology). The degree of molar substitution of the HES solution was determined and verified in duplicate according to the method described by Hodges \textit{et al.}\textsuperscript{16} and Lee \textit{et al.}\textsuperscript{17}

\textit{Experimental Protocol}

A total of 24 pigs underwent permuted block randomization for assignment to the study group (n = 12), receiving HES 650/0.42, or the control group (n = 12), receiving HES 130/0.42. The HES solutions were blinded to the experimental investigators and labeled K (HES 650/0.42) and L (HES 130/0.42). After all surgical preparations were completed, the animals were allowed to
recover for 45 min before the investigational protocol was started. Progressive acute normovolemic hemodilution was induced by steps of 10 ml \( \cdot \) kg\(^{-1} \cdot \) BW\(^{-1} \) with a 1:1 exchange of blood with either HES 650/0.42 or HES 130/0.42 until a total exchange of 50 ml \( \cdot \) kg\(^{-1} \cdot \) BW\(^{-1} \) was reached. The HES solution was injected into the right internal jugular vein at the same time and the same rate that blood was removed from the left carotid artery. Every hemodilutional step was conducted over exactly 30 min. At baseline and after each step of 10 ml \( \cdot \) kg\(^{-1} \cdot \) BW\(^{-1} \) blood exchange, citrated blood samples were obtained.

**Laboratory Measurements**

**TEG® Analysis.** The TEG® was used to assess the process of blood coagulation by testing the kinetics of the whole coagulation process.\(^\text{18} \) It has been shown previously that TEG® in conjunction with standard coagulation assays provides a complementary approach suitable for detection of coagulation abnormalities in the course of hemodilution by colloids.\(^\text{7,15} \) Technical details of the TEG® coagulation analyzer, performance of coagulation tests, and definition of the measured parameters have been described previously.\(^\text{18,19} \)

Thromboelastograph analysis was performed using two computerized TEG® 5000 coagulation analyzers. Blood samples were incubated for 1 h in a 37°C water bath,\(^\text{18,20} \) followed by blood recalcification and TEG® analysis according to the manufacturer’s instructions. The following TEG® parameters were reported: reaction time (r), coagulation time (k), maximal amplitude (MA), angle \( \alpha \), clot firmness (G), and coagulation index.\(^\text{18,20,21} \)

**Hemoglobin Concentration.** Arterial blood samples were collected using heparinized syringes (BD Preset; BD Vacutainer Systems, Plymouth, United Kingdom). Hemoglobin concentration was determined immediately after collection using the Rapidlab 865 analyzer (Bayer Vital GmbH, Fernwald, Germany).

For further laboratory measurements, blood samples were immediately centrifuged at 3,000 rpm for 15 min at 4°C for separation of plasma and blood cellular components (Rotanta/RP; Hettich, Bäch, Switzerland).

**Plasmatic Coagulation.** Prothrombin time (PT) and activated partial thromboplastin time (aPTT) were determined on an automated coagulation analyzer (BCS; Dade Behring, Marburg, Germany) using a PT reagent containing recombinant tissue factor (Innovin; Dade Behring) and an aPTT reagent containing ellagic acid (Actin FS; Dade Behring), respectively. Functional activity of vWF was determined in a commercial ristocetin-cofactor assay (vWF RCA; Dade Behring) on an automated coagulation analyzer (BCS; Dade Behring). Briefly, vWF activity was assessed by the ability to agglutinate fixed human platelets in the presence of ristocetin. Agglutination was measured turbidimetrically using the coagulation analyzer. FVIII was assessed functionally using factor VIII-deficient plasma (Dade Behring) according to the manufacturer’s instructions.

**Blood and Plasma Viscosity.** Measurement was performed immediately after collection using the plate cone technique at 38°C for linear increasing shear rates from 1 to 900 s\(^{-1} \) in 3 min (Rheostress1; Thermo Haake, Karlsruhe, Germany). Mean viscosities at shear rates from 300 to 900 s\(^{-1} \) were analyzed.

**HES Concentration.** Hydroxyethyl starch concentration was quantified after extraction from plasma and urine, respectively, and hydrolysis to glucose monomers. Briefly, plasma and urine samples (1 ml) were incubated at 100°C for 60 min after addition of 0.5 ml KOH solution 35% (wt/wt) (Fluka, Buchs, Switzerland). HES was precipitated by adding of 10 ml ice-cold absolute ethanol (Fluka) to the supernatant of the reaction mixture and acidly hydrolyzed in 2N HCl (Fluka) for 60 min at 100°C. Glucose determination was performed using an enzymatic test kit based on hexokinase/glucose 6-phosphatase (Boehringer Mannheim, Darmstadt, Germany). For determination of HES molecular weight, plasma proteins were eliminated by trichloroacetic acid precipitation (6.4% [wt/wt] end concentration) and neutralized supernatants were analyzed by GPC-MALLS (Wyatt Technology) at a flow rate of 1 ml/min in 70 ms phosphate buffer pH 7.0 using serial GPC columns HEMA Bio 40, 100, and 1000 (PS).

**Data Analysis**

The effects of the high-molecular-weight HES solution (650/0.42) on blood coagulation were compared with those of the low-molecular-weight HES solution (130/0.42) using a two-way analysis of variance for repeated measures (with and without baseline correction) on one way (dilution) with Greenhouse-Geisser correction for assessing solution and dilution effects and their interaction (JMP 5.1 statistical package; SAS Institute, Inc., Cary, NC).

Pharmacokinetic parameters were obtained through individual fitting of the plasma concentration data using the following model of exponential accumulation: Concentration = \( C_{ss} \cdot (1 - \exp(-\lambda \cdot \text{time})) \) (\( C_{ss} \) = concentration at steady state; \( \lambda \) = accumulation rate constant). This simple model was considered appropriate to fit the study data, which consisted only of isolated concentration values measured before and immediately after each hemodilutional step. The two parameters of the model were expected to be indirectly related with the true pharmacokinetic parameters of the infused products, i.e., \( C_{ss} \) reflects mainly the clearance and \( \lambda \) reflects mainly the half-life. Thus, a clearance-like parameter (CL) could be derived from \( C_{ss} \) (\( CL = \text{Dose per dilution unit/} C_{ss} \)), and a distribution volume-like parameter (V) could be derived from \( \lambda \) and CL (\( V = CL/\lambda \)). In addition, the excretion recovery of the colloids, expressed as a percentage of the cumulated dose infused throughout the experiment, was calculated using the urinary concentration and volume values. Here again, the obtained
value must be considered as only indirectly related to the true recovery value characterizing the colloids, because the experiment was interrupted before the completion of renal excretion. Because of the approximate model used for fitting, the obtained parameters must not be considered as true pharmacokinetic constants characterizing the colloids. However, under the assumption of roughly similar biases, comparisons between the two colloid solutions tested were possible.

Pharmacodynamic parameters were obtained through the individual fitting of concentration–effect relations, using a simple instantaneous linear model, relating the observed effect to the observed concentration values (C_obs): Thus, for each pharmacodynamic variable, a slope (corresponding to the change of the respective parameter in relation to HES plasma concentration) and an intercept (baseline effect for a zero concentration) were obtained. In a second step, the observed effect was related to the observed HES in vivo molecular weight again; for each pharmacodynamic variable, a slope (corresponding to the change of the respective parameter in relation to HES in vivo molecular weight) and an intercept (baseline effect for a zero HES in vivo molecular weight) were obtained.

Pharmacokinetic and pharmacodynamic parameters obtained from model fitting were thereafter compared between treatments by way of an unpaired Student t test. \( P < 0.05 \) (two-tailed) was considered statistically significant. A sample size determination was performed by a power analysis using data (TEG® parameters MA and angle \( \alpha \)) of a previously published in vivo study.\(^{15} \) A sample size of 12 animals per group was calculated to ensure 80% power with an estimated delta of 7.5% and an SD of 5%. Results are expressed as mean ± SD.

**Results**

No significant differences were found among the HES 650/0.42 and HES 130/0.42 groups with regard to BW and the following variables at baseline: coagulation parameters (TEG® and plasmatic coagulation), hemoglobin concentration, and viscosity (\( P > 0.05 \) for all).

**Coagulation Analyses**

**Plasmatic Coagulation.** Blood coagulation was increasingly compromised by progressive hemodilution with both HES solutions. A significant dilution effect toward hypocoagulability for all plasma coagulation parameters (PT, aPTT, FVIII activity, and vWF activity) was seen (\( P < 0.01 \) for all) (figs. 1A–D). On the basis of the baseline-corrected plasma coagulation parameters, HES 650/0.42 showed a significantly greater impact on aPTT compared with HES 130/0.42 (\( P = 0.04 \)) (figs. 1B and table 1), whereas PT (\( P = 0.99 \)), functional FVIII activity (\( P = 0.15 \)), and functional vWF activity (\( P = 0.19 \)) did not significantly differ from HES 130/0.42 (figs. 1A, C, and D and table 1).

**TEG®.** Except for \( r \), all TEG® parameters showed a significant dilution dependency toward hypocoagulability after infusion of the respective HES solution (\( P < 0.01 \) for all) (figs. 2A–F). On the basis of the baseline-corrected TEG® parameters, a significantly stronger decrease of MA (\( P = 0.04 \)), angle \( \alpha \) (\( P = 0.02 \)), and coagulation index (\( P = 0.02 \)) was seen after progressive
hemodilution with HES 650/0.42 as compared with HES 130/0.42 (figs. 2C, D, and F and table 1). No significant between-group differences were found for r (P = 0.11), k (P = 0.09), and G (P = 0.28) (figs. 2A, B, and E and table 1).

Hemoglobin Course

The hemoglobin concentration decreased similarly from 9.1 ± 0.8 g/dl to 4.6 ± 0.7 g/dl (HES 650/0.42) and from 9.0 ± 0.4 g/dl to 4.8 ± 0.4 g/dl (HES 130/0.42) after acute normovolemic hemodilution with the respective solution (P < 0.01) (fig. 3A).

Viscosity

Hemodilution with both HES solutions significantly decreased blood viscosity (P < 0.01). Plasma viscosity shows a downward trend after acute normovolemic hemodilution with the respective solution (P = 0.06). However, no significant intergroup differences were seen (P = 0.53 for blood viscosity and P = 0.90 for plasma viscosity) (figs. 3B and C).

Table 1. Changes of Coagulation Parameters during Acute Normovolemic Hemodilution (50 ml/kg)

<table>
<thead>
<tr>
<th>Parameters</th>
<th>HES 650/0.42 (n = 12)</th>
<th>HES 130/0.42 (n = 12)</th>
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</thead>
<tbody>
<tr>
<td>Coagulation parameters</td>
<td></td>
<td></td>
</tr>
<tr>
<td>PT, s</td>
<td>2.09 ± 0.75†</td>
<td>1.88 ± 0.46</td>
</tr>
<tr>
<td>aPTT, s</td>
<td>6.25 ± 2.93*</td>
<td>4.25 ± 2.60</td>
</tr>
<tr>
<td>FVIII, %</td>
<td>–328 ± 34‡</td>
<td>–272 ± 102</td>
</tr>
<tr>
<td>vWF, %</td>
<td>–11.5 ± 8.2†</td>
<td>–7.8 ± 7.9</td>
</tr>
<tr>
<td>TEG® parameters</td>
<td></td>
<td></td>
</tr>
<tr>
<td>r, mm</td>
<td>0.95 ± 1.28†</td>
<td>0.33 ± 1.86</td>
</tr>
<tr>
<td>k, mm</td>
<td>0.38 ± 0.36†</td>
<td>0.17 ± 0.23</td>
</tr>
<tr>
<td>MA, mm</td>
<td>–10.79 ± 3.65‡</td>
<td>–8.22 ± 2.98</td>
</tr>
<tr>
<td>angle α, °</td>
<td>–5.94 ± 1.81*</td>
<td>–2.48 ± 3.26</td>
</tr>
<tr>
<td>G, dyne/cm²</td>
<td>–5.738 ± 2.3111‡</td>
<td>–4.635 ± 2.297</td>
</tr>
<tr>
<td>Coagulation index</td>
<td>–2.18 ± 0.85*</td>
<td>–1.35 ± 1.13</td>
</tr>
</tbody>
</table>

Data are mean ± SD.

* P < 0.05 vs. hydroxyethyl starch (HES) 130/0.42. † Not significant (P > 0.05) vs. HES 130/0.42.

aPTT = activated partial thromboplastin time; FVIII = functional activity of factor VIII; G = clot firmness; k = coagulation time; MA = maximal amplitude; PT = prothrombin time; r = reaction time; vWF = functional activity of von Willebrand factor.

Fig. 2. Effect of progressive acute normovolemic hemodilution with hydroxyethyl starch (HES) 650/0.42 (n = 12) and HES 130/0.42 (n = 12) on the main TEG® parameters (reaction time [r; A], coagulation time [k; B], maximal amplitude [MA; C], angle α [D], clot firmness [G; E], and coagulation index [CI; F]). TEG® parameters were determined before (baseline [BL]) and immediately after each step of acute normovolemic hemodilution (10, 20, 30, 40, and 50 ml/kg body weight). Results are mean ± SD. Solution effect (Psol) and dilution effect (Pdil) of HES 650/0.42 versus HES 130/0.42 as well as interaction between treatment and dilution (Psol × dil) as determined by two-way analysis of variance for repeated measurements on one way (dilution).
Hydroxyethyl starch plasma concentration increased significantly over the whole experimental period after hemodilution with the respective HES solution (P < 0.01 for both), showing higher plasma concentrations for HES 650/0.42 (9.6 ± 1.0 g/l) as compared with HES 130/0.42 (7.3 ± 0.9 g/l) (P < 0.01) (fig. 4A). Mean in vivo molecular weight increased progressively over the whole experimental period after hemodilution with the respective solution (P < 0.01), resulting in higher values for HES 650/0.42 (32.3 ± 2.7 kd) as compared with HES 130/0.42 (21.8 ± 2.5 kd) (P < 0.01) (fig. 4B). The extrapolated HES concentration at steady state (Css) was significantly higher for HES 650/0.42 (10.2 ± 1.2 g/l) as compared with HES 130/0.42 (7.7 ± 1.2 g/l) (P < 0.01) (table 2).

The pharmacokinetic analysis revealed the following treatment effects (table 2): highly significant intergroup differences were found regarding total clearance (CL) and volume of distribution (V), showing smaller values for HES 650/0.42 as compared with HES 130/0.42 (P < 0.01 for all). No significant differences between both treatments appeared regarding the accumulation rate constant (λ) and urinary recovery (P > 0.50).

**HES Pharmacokinetics**

Hydroxyethyl starch plasma concentration increased significantly over the whole experimental period after hemodilution with the respective HES solution (P < 0.01 for both), showing higher plasma concentrations for HES 650/0.42 (9.6 ± 1.0 g/l) as compared with HES 130/0.42 (7.3 ± 0.9 g/l) (P < 0.01 for both), showing higher plasma concentrations for HES 650/0.42 (9.6 ± 1.0 g/l) as compared with HES 130/0.42 (7.3 ± 0.9 g/l) (P < 0.01 for both).
Concentration–Effect Analysis

The concentration curve of the HES solutions was adequately fitted by the instantaneous linear model used in this study as demonstrated by the excellent correlation between observed versus predicted plasma concentrations ($r^2 = 0.984$) (fig. 5A). In addition, the applicability of the model used was confirmed by the absence of marked trend across the whole concentration range in the Bland-Altman analysis (fig. 5B).

When relating the observed effect with the measured plasma concentration of HES (table 3), no significant differences between HES 650/0.42 and HES 130/0.42, regarding the TEG® parameters ($P > 0.05$ for all; $r [P = 0.75], k [P = 0.73], MA [P = 0.43], angle $α$ [P = 0.67], $G [P = 0.21]$, and coagulation index $[P = 0.71]$) were seen (fig. 6A). Except $FVIII$ ($P = 0.04$), no significant differences with the plasmatic coagulation parameters after comparison of HES 650/0.42 with HES 130/0.42 were found ($PT [P = 0.23], aPTT [P = 0.79], vWF [P = 0.63]$) (fig. 6B). The decrease in hemoglobin concentration ($P = 0.03$) (fig. 6C and table 3) was less pronounced after progressive hemodilution with HES 650/0.42 as compared with HES 130/0.42.

When relating the observed effect with the measured HES in vivo molecular weights, no significant differences between HES 650/0.42 and HES 130/0.42 regarding the TEG® parameters ($P > 0.05$ for all; $r [P = 0.93], k [P = 0.63], MA [P = 0.69], angle $α$ [P = 0.97], $G [P = 0.26]$, and coagulation index $[P = 0.86]$) (fig. 6D) as well as plasmatic coagulation were found ($P > 0.05$ for all; $PT [P = 0.39], aPTT [P = 0.54], FVIII [P = 0.17], vWF [P = 0.58]$) (fig. 6E). The decrease in hemoglobin concentration ($P = 0.20$) (fig. 6F) did not significantly differ after progressive hemodilution with HES 650/0.42 as compared with HES 130/0.42. The consistently higher

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**Table 2. Pharmacokinetic Parameters**

<table>
<thead>
<tr>
<th>Pharmacokinetic Parameters</th>
<th>HES 650/0.42 (n = 12)</th>
<th>HES 130/0.42 (n = 12)</th>
</tr>
</thead>
<tbody>
<tr>
<td>HES concentration at steady state, g/l</td>
<td>10.2 ± 1.2*</td>
<td>7.7 ± 1.2</td>
</tr>
<tr>
<td>Clearance, l/min</td>
<td>0.084 ± 0.012*</td>
<td>0.114 ± 0.020</td>
</tr>
<tr>
<td>Accumulation rate constant, min⁻¹</td>
<td>0.012 ± 0.002†</td>
<td>0.012 ± 0.003</td>
</tr>
<tr>
<td>Volume of distribution, l</td>
<td>7.39 ± 1.39*</td>
<td>9.51 ± 1.37</td>
</tr>
<tr>
<td>Urinary recovery, %</td>
<td>5.73 ± 4.73†</td>
<td>8.94 ± 5.25</td>
</tr>
</tbody>
</table>

Data are mean ± SD.
* $P < 0.05$ vs. hydroxyethyl starch (HES) 130/0.42. † Not significant ($P > 0.05$) vs. HES 130/0.42.

**Table 3. Pharmacodynamic Parameters**

<table>
<thead>
<tr>
<th>Pharmacodynamic Parameters</th>
<th>Changes per g/l Plasma Concentration</th>
</tr>
</thead>
<tbody>
<tr>
<td>HES 650/0.42 (n = 12)</td>
<td>HES 130/0.42 (n = 12)</td>
</tr>
<tr>
<td>r, mm</td>
<td>0.08 ± 0.10†</td>
</tr>
<tr>
<td>k, mm</td>
<td>0.03 ± 0.02†</td>
</tr>
<tr>
<td>MA, mm</td>
<td>−1.12 ± 0.26†</td>
</tr>
<tr>
<td>angle $α$, °</td>
<td>−0.59 ± 0.17†</td>
</tr>
<tr>
<td>$G$, dyne/cm²</td>
<td>−598 ± 190†</td>
</tr>
<tr>
<td>Coagulation index</td>
<td>−0.22 ± 0.05†</td>
</tr>
<tr>
<td>$PT$, s</td>
<td>0.20 ± 0.07†</td>
</tr>
<tr>
<td>aPTT, s</td>
<td>0.61 ± 0.21†</td>
</tr>
<tr>
<td>$FVIII$, %</td>
<td>−34.4 ± 3.3*</td>
</tr>
<tr>
<td>vWF, %</td>
<td>−1.34 ± 0.86†</td>
</tr>
<tr>
<td>Hb, g/dl</td>
<td>−0.48 ± 0.07*</td>
</tr>
</tbody>
</table>

Changes of the respective coagulation and TEG® parameters as well as hemoglobin per g/l plasma concentration of hydroxyethyl starch (HES) 650/0.42 and HES 130/0.42, respectively. The concentration-effect relation can be characterized by the extent of the decrease/increase in the respective parameter per g/l (i.e., the more negative the number is in the table, the greater is the decrease of the respective parameter per g/l plasma concentration of HES; the more positive the number is in the table, the greater is the increase of the respective parameter per g/l plasma concentration of HES). Data are mean ± SD.
* $P < 0.05$ vs. HES 130/0.42. † Not significant ($P > 0.05$) vs. HES 130/0.42.

$PT$ = activated partial thromboplastin time; $FVIII$ = functional activity of factor $VIII$; $G$ = clot firmness; $Hb$ = hemoglobin; $k$ = coagulation time; $MA$ = maximal amplitude; $PT$ = prothrombin time; $r$ = reaction time; $vWF$ = functional activity of von Willebrand factor.

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Anesthesiology, V 105, No 6, Dec 2006

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vivo molecular weights during the whole experimental period after hemodilution with HES 650/0.42 (n = 12) and HES 130/0.42 (n = 12), respectively (A–C). Relation of the measured HES molecular weight to the observed effects during acute normovolemic hemodilution with HES 650/0.42 (n = 12) and HES 130/0.42 (n = 12), respectively (D–F). * P < 0.05 for the slope of HES 650/0.42 versus HES 130/0.42. ns = not significant (P > 0.05) for the slope of HES 650/0.42 versus HES 130/0.42. aPTT = activated partial thromboplastin time; Cl = coagulation index; Hb = hemoglobin concentration.

Discussion

High-molecular-weight HES (650/0.42) shows a moderately greater antihemostatic effect than low-molecular-weight HES (130/0.42) when administered in equal doses during acute normovolemic hemodilution. However, similar effects on hemostasis were observed with both HES solutions when the observed blood coagulation-impairing effects were related to the measured HES plasma concentrations.

Hydroxyethyl starches are polydisperse solutions with a wide variety of physicochemical characteristics in terms of mean molecular weight, degree of substitution, and C2/C6 ratio accounting for their pharmacokinetic and pharmacodynamic behavior in vivo.1,2,22 The interference with blood coagulation as a major adverse effect after HES administration has repeatedly been described and may be regarded as a serious limitation to their clinical use.22 Numerous former studies postulated molecular weight being responsible for the observed antihemostatic effects.1,7,9,13,14,23–25 However, the main limitation of these studies consisted of a concomitant reduction in molecular weight and molar substitution. Recently, Madjdpour et al.15 have scrutinized the isolated effect of molecular weight on blood coagulation, showing that low-substituted high-molecular-weight HES (500/0.4 and 900/0.4) influences plasmatic blood coagulation similarly as low-substituted low-molecular-weight HES (130/0.4). Therefore, a high-molecular low-substituted HES solution is expected to show an improved pharmacokinetic behavior with a prolonged initial half-life without an exaggerated compromise on blood coagulation.

Based on these findings, the current study reassessed the blood coagulation-impairing effect of low-substituted high-molecular-weight HES (650/0.42) as compared with low-substituted low-molecular-weight HES (130/0.42) during a clinically more relevant model, i.e., progressive acute normovolemic hemodilution. The impact on hemostasis of the two colloids was analyzed by means of TEG® and plasmatic coagulation tests.
Most of the TEG® parameters (figs. 1A–D) as well as all plasmatic coagulation tests (figs. 2A–F) significantly worsened toward hypocoagulability during progressive acute normovolemic hemodilution with the tested solutions. A more pronounced deterioration of TEG® parameters as demonstrated by decreased clot strength (angle α and maximal amplitude) as well as coagulation index has been observed with HES 650/0.42 as compared with HES 130/0.42 (figs. 2C, D, and F and table 1). Regarding plasmatic coagulation tests, the results were less pronounced: Only aPTT was significantly more prolonged with HES 650/0.42 as compared with HES 130/0.42 (fig. 1B and table 1). Because progressive normovolemic hemodilution (50 ml/kg) with HES 650/0.42 leads to higher plasma concentrations as compared with HES 130/0.42 (fig. 4A), a subsequent concentration-effect analysis relating the observed effect on blood coagulation with the measured plasma concentration of HES was effected. Except for FVIII, similar alterations of the coagulation parameters after HES 650/0.42 and HES 130/0.42 administration were observed (figs. 6A and B and table 3). These results indicate that the blood coagulation-impairing effect of HES solutions is directly governed by the plasma concentration and thus related to the administered volume. In addition, a further analysis relating the observed effects to the measured HES in vivo molecular weights confirmed that molecular weight was not the crucial factor for the observed blood coagulation-compromising effect (figs. 6D and E).

The significantly higher in vivo mean molecular weight of HES 650/0.42 as compared with HES 130/0.42 (fig. 4B) seems to result in a lesser extravasation and slower disappearance rate of HES 650/0.42 (table 2), resulting in higher plasma concentrations of HES 650/0.42 as compared with HES 130/0.42 (fig. 4A). Given the volume of distribution and the calculated clearance of both tested HES solutions (table 2), similar elimination half-lives have been found.

Hemoglobin concentration may be used as endogenous point attractor for indirect illustration of the volume effect of infused colloids. Acute normovolemic hemodilution with the respective solution leads to a significant reduction in hemoglobin concentrations (50% by HES 650/0.42 and 46% by HES 130/0.42) showing no significant intergroup differences (fig. 3A). When relating the decrease in hemoglobin concentration to the measured plasma concentration of HES, a significantly lesser decrease of hemoglobin concentration has been described with HES 650/0.42 as compared with HES 130/0.42 (fig. 6C and table 3). However, no significant differences after hemodilution with HES 650/0.42 as compared with HES 130/0.42 have been observed by relating the decrease in hemoglobin concentration to the measured HES in vivo molecular weights (fig. 6F). The volume effect of HES solutions depends on the circulating number of osmotically active molecules.2,3 The exaggerated decrease of the hemoglobin concentration during acute normovolemic hemodilution with HES 130/0.42 thus may indicate that more molecules were present than during acute normovolemic hemodilution with HES 650/0.42. This may indeed be the case because the plasma concentration of HES 650/0.42 was only 32% higher than the plasma concentration of HES 130/0.42 (fig. 4A), whereas the mean molecular weight of HES 650/0.42 was 48% higher than the mean molecular weight of HES 130/0.42 (fig. 4B). Accordingly, our findings may indicate less effective plasma volume restoration in relation to the plasma concentration of HES 650/0.42 as compared with HES 130/0.42.

Blood rheology has shown to be improved by various mechanisms after HES administration.26,27 The predominant rheologic effect of colloids consists in the reduction of whole blood viscosity proportional to the magnitude of their plasma volume expansion.27 Plasma viscosity, however, is determined principally by the number and physical properties of dissolved macromolecules.27 Accordingly, progressive acute normovolemic hemodilution with HES 650/0.42 and HES 130/0.42, respectively, leads to improved rheologic conditions by demonstrating a significant decrease of whole blood viscosity (24%) as well as a strong downward trend of plasma viscosity (6%) (figs. 3B and C). However, no significant differences between the tested solutions were found.

The pig is a suitable animal model for blood coagulation research.28 It has been used to monitor coagulation changes under various circumstances, such as in normovolemic hemodilution, supraceliac aortic cross-clamping, and hemorrhagic shock.29–31 Commercially available coagulation tests, functional hemostatic assays, and thromboelastograph analysis (ROTEM; Pentapharm Ltd., Basel, Switzerland) have been shown to be applicable for porcine blood.32,33 More importantly, McLoughlin et al.29 have shown that the response of PT and aPTT to profound hemodilution is similar in humans and pigs. Porcine coagulation thus reacts quite similarly to hemodilution with HES solutions as compared with the human coagulation system. Nevertheless, precautions must be taken in interpretation of the results as well as in their extrapolation toward human results.33 Therefore, in the current study, the known hypercoagulability of the pig may have masked the deleterious effects of both treatments regarding the coagulation parameters, which could have occurred with other species, i.e., humans. Furthermore, no standard platelet aggregation tests have been included in this study, and TEG® may not be adequately sensitive in detecting platelet-related changes in aggregability and function.

Several further limitations of the current study must be considered. Because the current study was not designed for pharmacokinetic analyses, only an approximate pharmacokinetic model was applicable. Therefore, the con-
clusions drawn by this model involve several assumptions and future studies are necessary to confirm our preliminary findings. In addition, investigation of adverse side effects (i.e., impairment of blood coagulation) of high- and low-molecular-weight low-substituted HES solutions in further clinical settings (acute vs. chronic vs. repetitive administration) are desirable to evaluate their clinical utility. Besides the extensively described volume restoring properties, HES seems to exert significant beneficial antiinflammatory effects,34,35 such as a diminished polymorphonuclear neutrophil sequestration in multiple organs.36 Recent studies have shown that the clinically relevant effect of HES on leukocyte sequestration depends on the regulation of the integrin function.36 The duration of the antiinflammatory effect after HES administration thus may be largely determined by the intravascular elimination of the colloid.36 Contrary to these findings, no effect or an apparent proinflammatory action after HES administration has recently been shown by Lang et al.37 Additional studies evaluating the antiinflammatory effect of high-molecular-weight low-substituted HES solutions due to their probable longer intravascular confinement thus seem to be worthwhile.

We conclude that high-molecular-weight HES (650/0.42) shows a moderately greater antihemostatic effect than low-molecular-weight HES (130/0.42) when administered in equal doses during acute normovolemic hemodilution. However, similar effects on hemostasis were observed with both HES solutions when the observed blood coagulation–impairing effects were related to the measured HES plasma concentrations. In addition, HES 650/0.42 may have a lower efficacy in immediately restoring plasma volume.

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